Nanoparticle-Augmented Sonodynamic Therapy

Literature Seminar 2020/6/1 Wataru Atsumi (B4)

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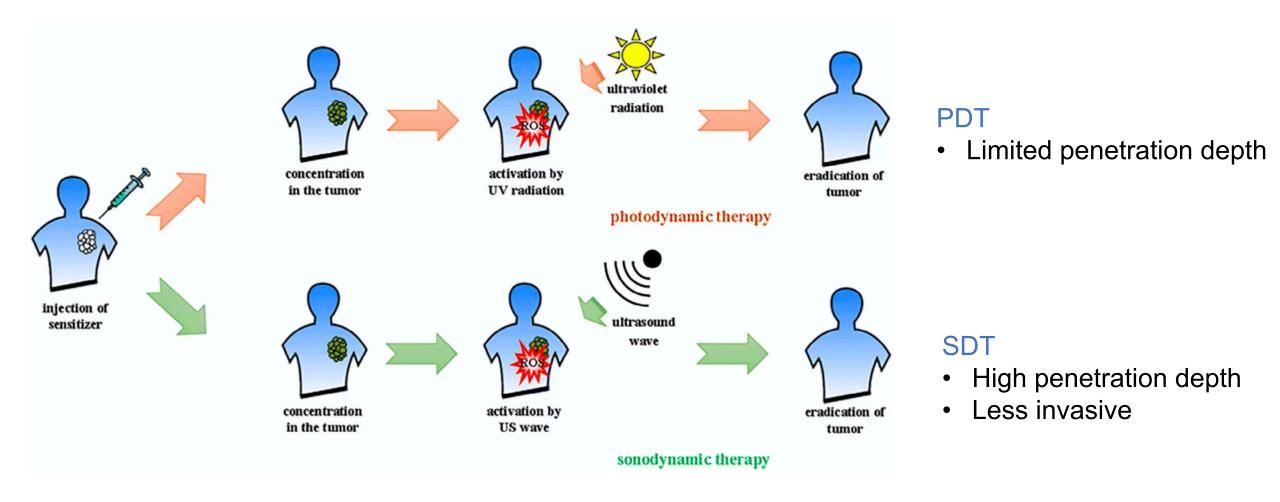
• Introduction

About sonodynamic therapy
Benefits of using nanoparticles

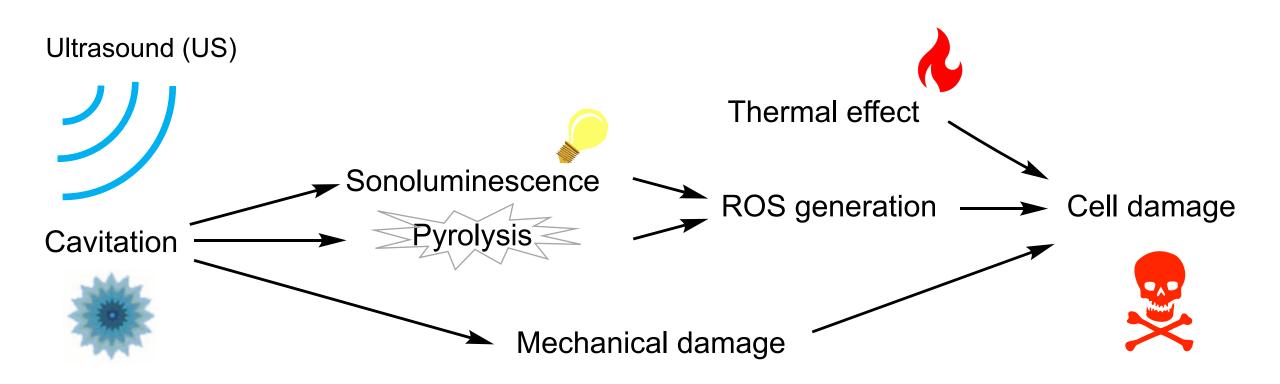
Examples of Nanoparticle-assisted SDT
 Self-assembled organic NPs
 NPs-assisted SDT for glioma
 NPs-assisted SDT for Alzheimer disease

Summary

Photodynamic therapy (PDT) & Sonodynamic therapy (SDT)



Schematic diagram of the possible mechanism of SDT



1. Cavitation

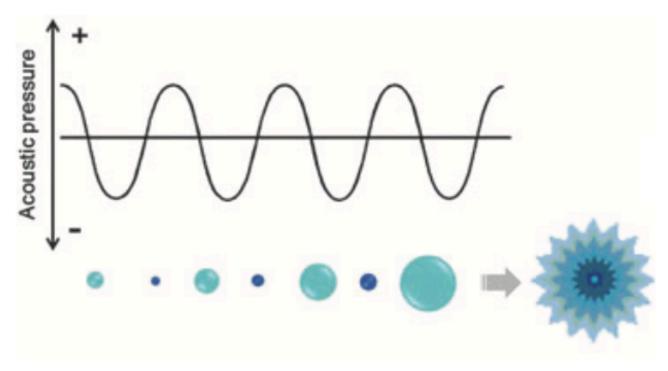


Figure 1 Drawing showing the formation, growth, and collapse of a cavitation bubble.

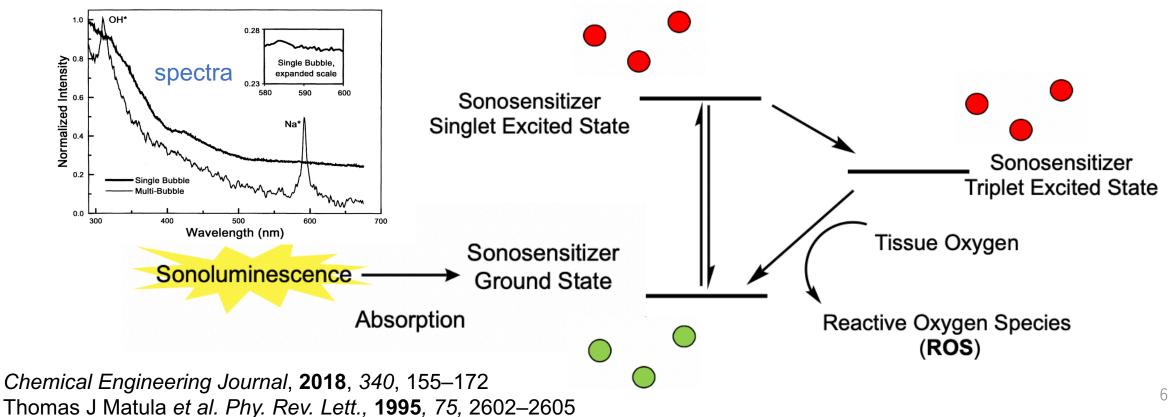
Cavitation has three stages.

- 1. Nucleation
- 2. Bubble growth
- 3. Implosive collapse

When it collapses, the local temperature and pressure can reach >10,000 K and 800 atm.

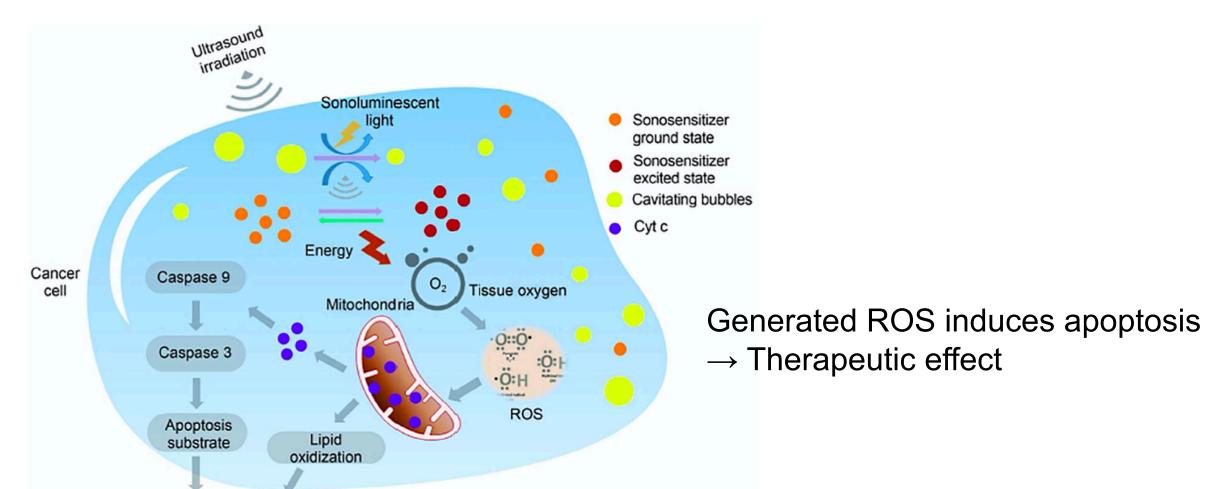
2. Sonoluminescence

- A concentration of energy caused by cavitation can generates light.
- Sonosensitizers are excited and generates ROS.



Cell apoptosis

3. Cellular toxicity by reactive oxygen species (ROS)



Chemical Engineering Journal, 2018, 340, 155–172

4. Other Effects

Pyrolysis of H₂O

Cavitation also induces pyrolysis of H₂O and generates ROS.

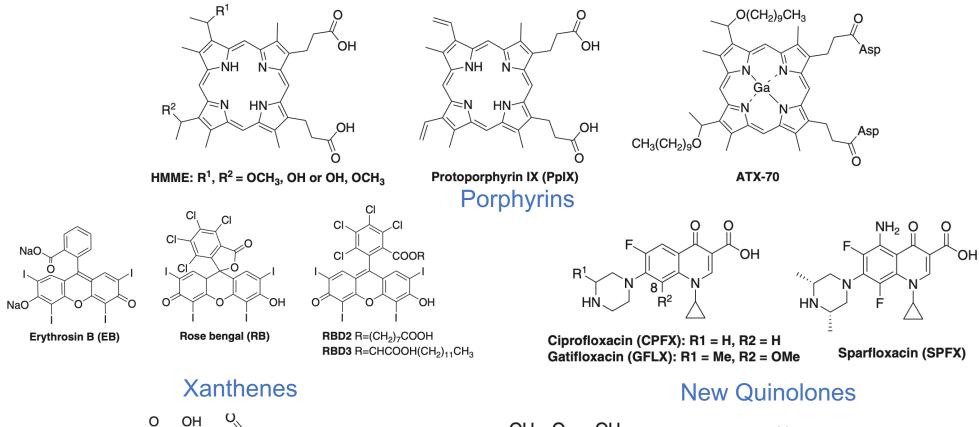
Mechanical damage

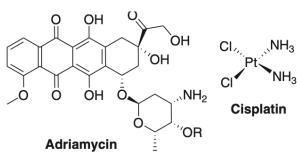
The strong shock waves are generated by cavitation, resulting in mechanical damage to the cell.

Thermal Effect

The transformation and absorption of US energy cause hyperthermia and induce necrosis.

Sonosensitizer





Drug Discovery Today, **2014**, *19*, 504–506

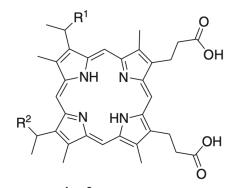
Antitumor drugs

Other types

9

Example of sonosensitizer

sonosensitizer: hematoporphyrin monomethyl ether (HMME)



HMME: R^1 , R^2 = OCH₃, OH or OH, OCH₃

Condition

Time: 60s

Frequency: 1MHz

Intensity: 1W/cm²

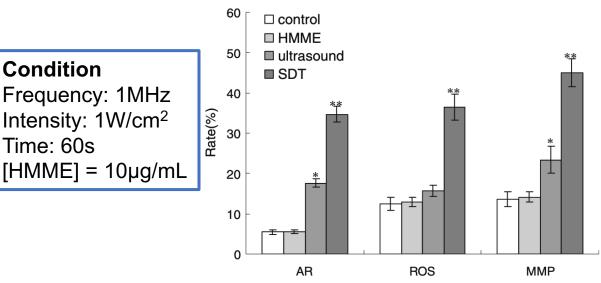


Fig. 2 Apoptotic rate (AR), ROS, and mitochondria membrane potential (MMP, means decreased MMP) of the C6 glioma cells after SDT, ultrasound, HMME, and no treatment by FCM.

ROS generation by HMME+US

- → Mitochondrial damage
- → Induction of apoptosis
- →Therapeutic effect for C6 glioma cells

SDT can be a valid way to treat cancer.

S. Dai, S. Hu, C. Wu, Acta Neurochir., **2009**, *151*, 1655 –1661.

Problems of traditional sonosensitizers

Because most of sonosensitizers are strongly hydrophobic, there are some problems as below.

- Low bioavailability
- Fast elimination out of the body
- Poor accumulation into targeted tissue

These problems hinder their clinical translation.

SDT augmented by nanoparticles (NPs)

Merits

- ✓ Large surface area suitable for chemical modification
- → Improvement of biocompatibility, biodistribution and selectivity
- ✓ Combination of SDT with other therapeutic modalities
- ✓ Decrease of cavitation threshold by NPs
- → Stabilization of nanobubbles on their surface and inside cavities
 - → Enhancement of the therapeutic efficiency

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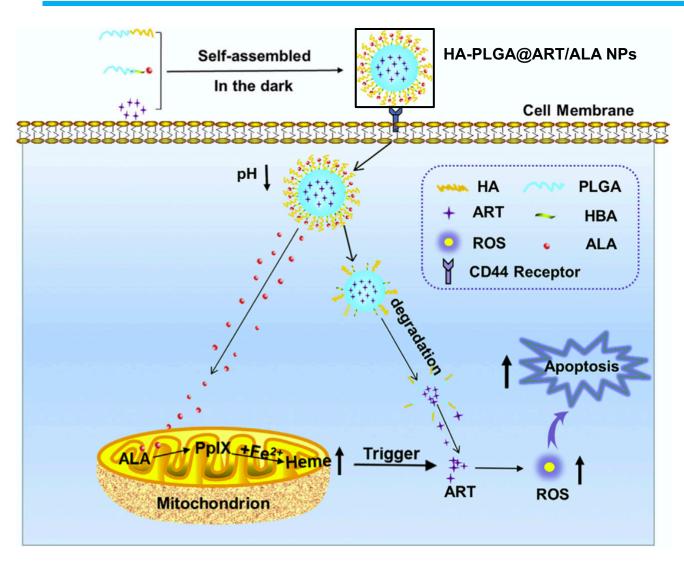
Self-assembled organic NPs

NPs-assisted SDT for glioma

NPs-assisted SDT for Alzheimer disease

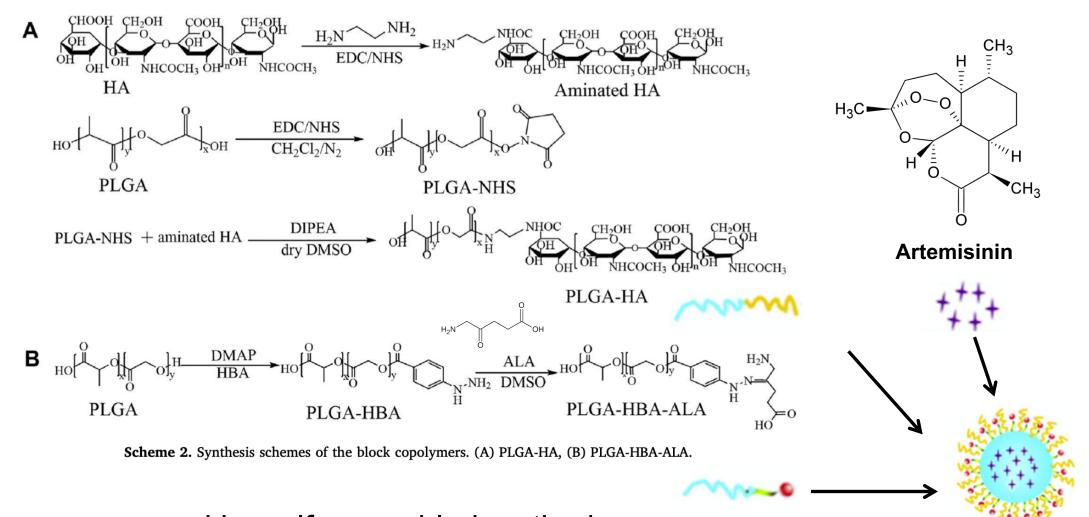
Summary

Self-assembled organic NPs



- Poly(lactic-co-glycolic acid) (PLGA):
 great biocompatibility and biodegradability
- Hyaluronic acid (HA):
 tumor-targeting
- 4-hydrazinobenzoic acid(HBA):
 pH-sensitive linkage
- Artemisinin (ART):
 ROS generation (as a sonosensitizer)
- Amino levulinic acid (ALA):
 precursor of Heme and activate ART (also as a sonosensitizer)

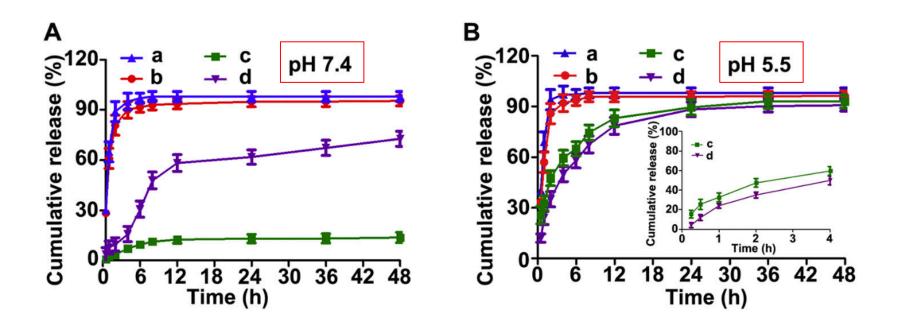
Structure of HA-PLGA@ART/ALA NPs



NP were prepared by self-assembled method. Hydrophobic ART was encapsulated in the inner core.

Lei Wang, et al. J. Controlled Release, **2018**, 286, 74–84.

In vitro pH-sensitive drug release assay



- a. free ALA
- b. free ART
- c. ALA from NPs
- d. ART from NPs

ALA were released under the acidic condition.

 At pH 5.5, ALA was released faster than ART, especially at the early time points.

Cytotoxicity and ROS production

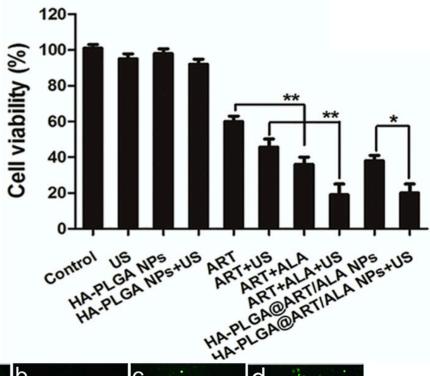
Condition

Intensity: 2 W/cm²

Time: 60 s

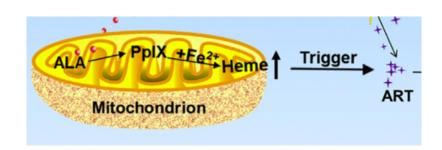
 $[ART] = 88 \mu M$

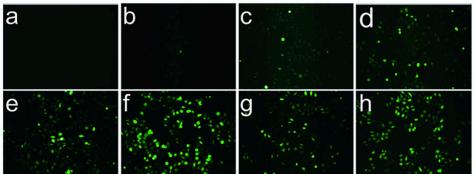
[ALA] = 0.5 mM



* More ROS generation by US

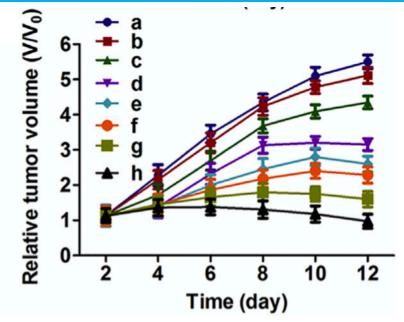
** Combination of ALA & ART

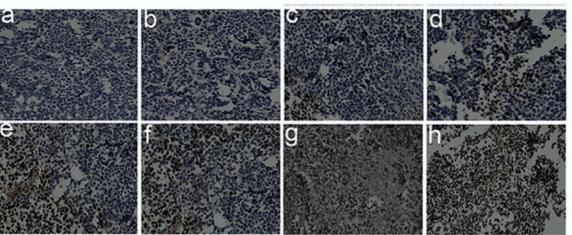




- a. Control e. ART+ALA
- b. US f. ART+ALA+US
- c. ART g. HA-PLGA@ART/ALA NPs
- d. ART+US h. HA-PLGA@ART/ALANPs NPs + US

Animal experiments





NPs + US group was the most effective.

- ✓ More drug accumulation by HA
- ✓ ART & ALA combination
- ✓ More ROS production by US

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a. Control e. ART+ALA
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b. US f. ART+ALA+US

c. ART g. HA-PLGA@ART/ALA NPs

d. ART+US h. HA-PLGA@ART/ALANPs NPs + US

Animal experiments

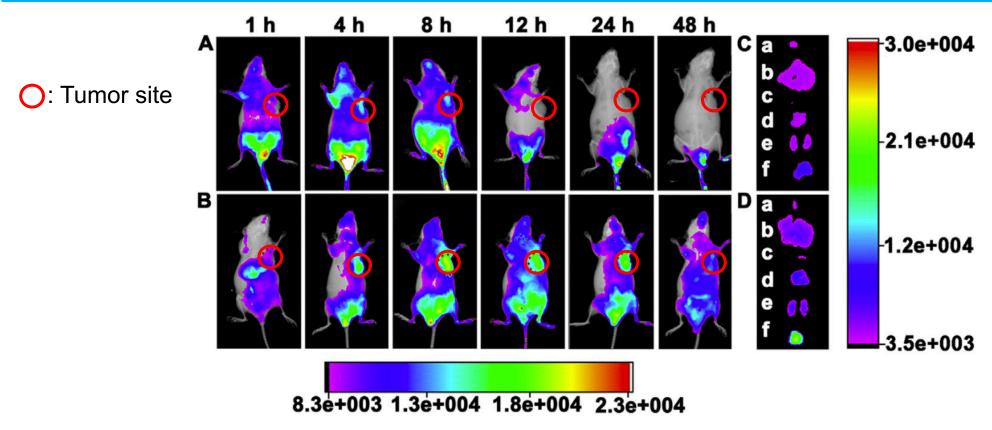


Fig. 7. *In vivo* NIR fluorescence imaging. Representative *in vivo* fluorescence images of tumor-bearing mice following tail vein administration of (A) IR780 and (B) HA-PLGA@IR780 NPs at different time points. *Ex vivo* NIR fluorescence images of major organs and tumors dissected from mice at 48 h after injection of (C) IR780 and (D) HA-PLGA@IR780 NPs: (a) heart, (b) liver, (c) spleen, (d) lung, (e) kidney, (f) tumor.

- ✓ Tumor targeting by HA
- ✓ Long circulation characteristic

Lei Wang, et al. J. Controlled Release, 2018, 286, 74-84.19

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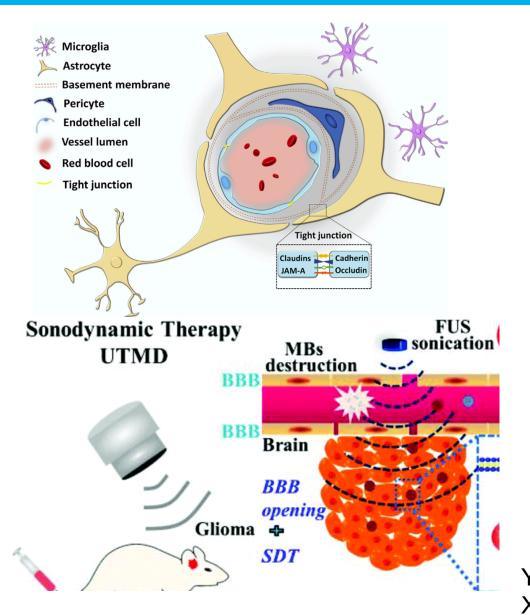
Self-assembled organic NPs

NPs-assisted SDT for glioma

NPs-assisted SDT for Alzheimer disease

Summary

BBB opening by microbubbles and US



BBB (blood-brain barrier) is the main obstacle to the drug delivery.

BBB can be opened up locally and reversibly by **Ultrasound-Targeted Microbubble Destruction (UTMD)**.

Yue Sun *et al. Biomater. Sci.,* **2019**, 7, 985–994. Ziaobing Wang *et al. Ultrason. Sonochem.,* **2017**, 37, 592–599

NPs-assisted SDT for glioma



DVDMS

- LiposomeDrug carrier
- DVDMS (Sinoporphyrin sodium)
 Hydrophilic sonosensitizer
- ανβ3 integrin
 Specifically expressed in tumor cells

NH N HN 4 Na

• iRGD $\alpha v \beta 3$ integrin-targeting peptide

BBB opening in vivo

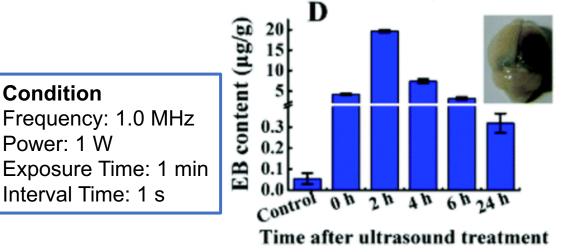
Content of Evans blue in the brain

Condition

Power: 1 W

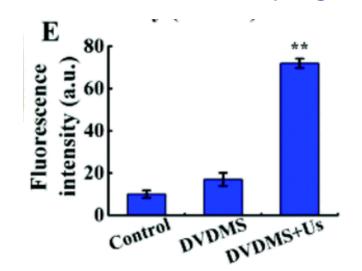
Frequency: 1.0 MHz

Interval Time: 1 s



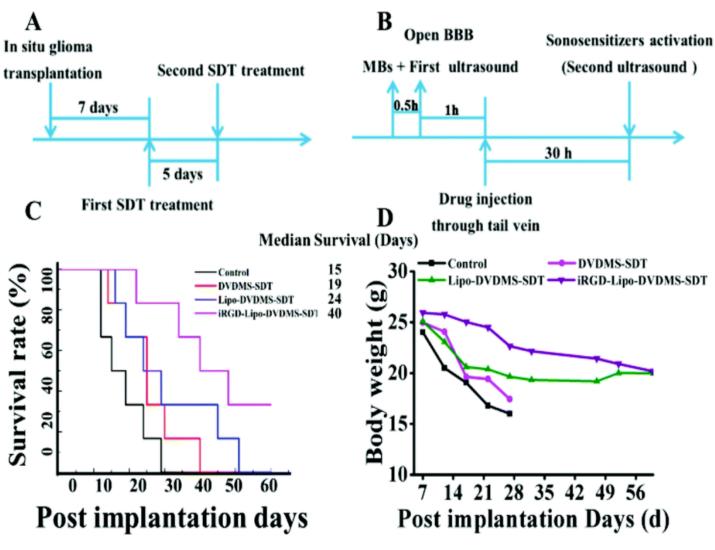
BBB showed the highest permeability 2h after UTMD.

DVDMS accumulation in orthotopic gliomas



The penetration of DVDMS with UTMD was 7.2-fold higher than that without UTMD.

Sonodynamic effect in vivo



Condition(UTMD)

Frequency: 1.0 MHz

Power: 1 W

Exposure Time: 1 min

Interval Time: 1 s

Condition (SDT)

Frequency: 1.0 MHz

Power: 1 W

Exposure Time: 1 min

Survival time of mice treated with iRGD-Lipo-DVDMS-SDT was longer than the others.

- √BBB opening
- √ tumor targeting by iRGD
- ✓DVDMS delivery by liposome

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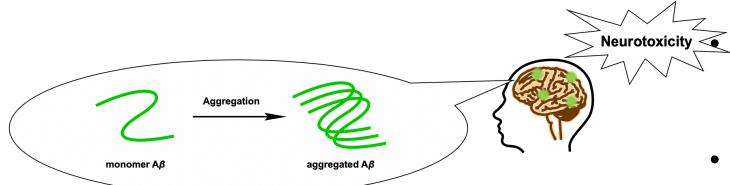
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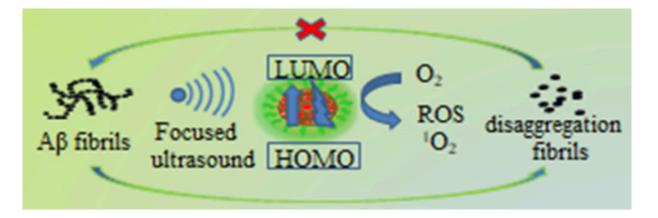
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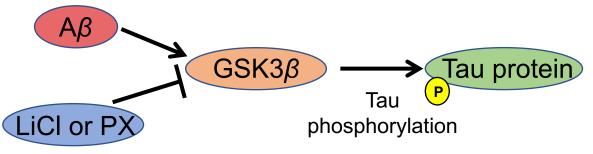
NPs-assisted SDT for Alzheimer disease

Summary

Alzheimer disease



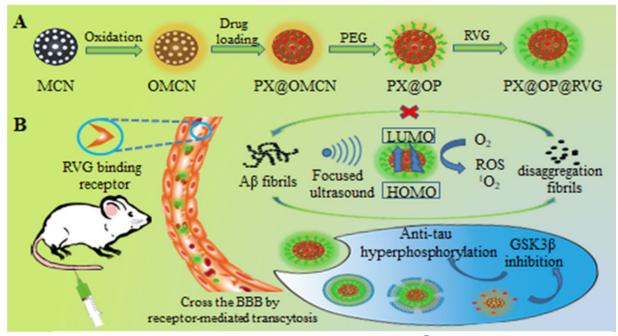




Aggregation of $A\beta$ is main cause of Alzheimer disease (AD).

- Oxygenation of Aβ by sonosensitizer with US may be a valid way to treat AD.
- Tau hyperphosphorylation is also a cause of AD.
- Inhibiting Glycoprotein synthase kinase-3 β (GSK3 β) is a hopeful treatment.

IX-modified multifunctional NPs



OH NH N OH OH

Protoporphyrin IX (PpIX)
Sonosensitizer

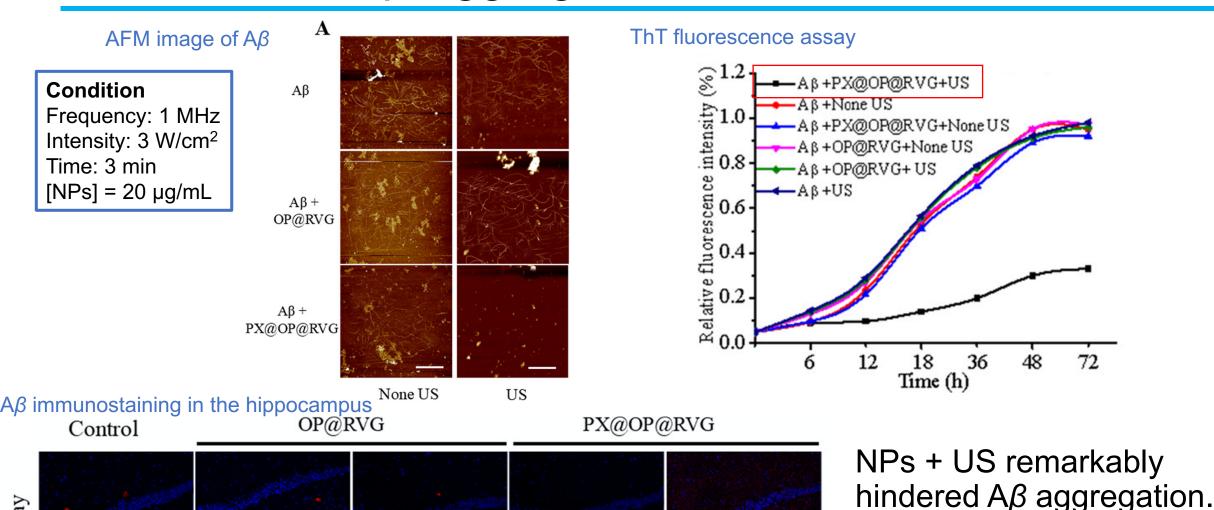
- Oxidized mesoporous carbon nanosphere (OMCN): drug carrier
- PpIX or PX: sonosensitizer and GSK3β inhibitor
- Rabies Virus Glycoprotein (RVG): It improves BBB penetration and selectivity of brain cell

Inhibition of $A\beta$ aggregation

US

None US/US

None US



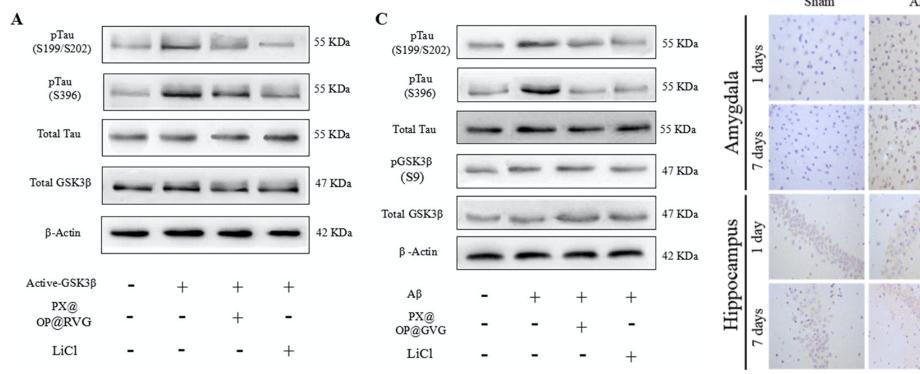
None US

US

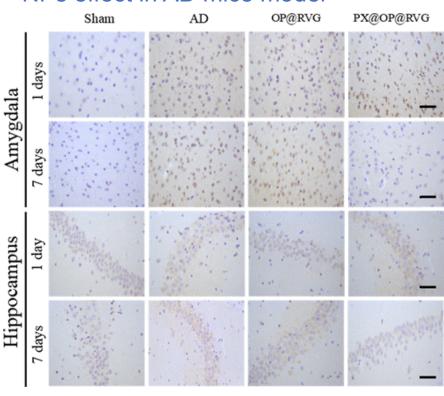
Mengmeng Xu *et al*. *ACS Appl. Mater. Interfaces*, ₂₈ **2018**, *10*, 32965–32980

Inhibition of tau hyperphosphorylation



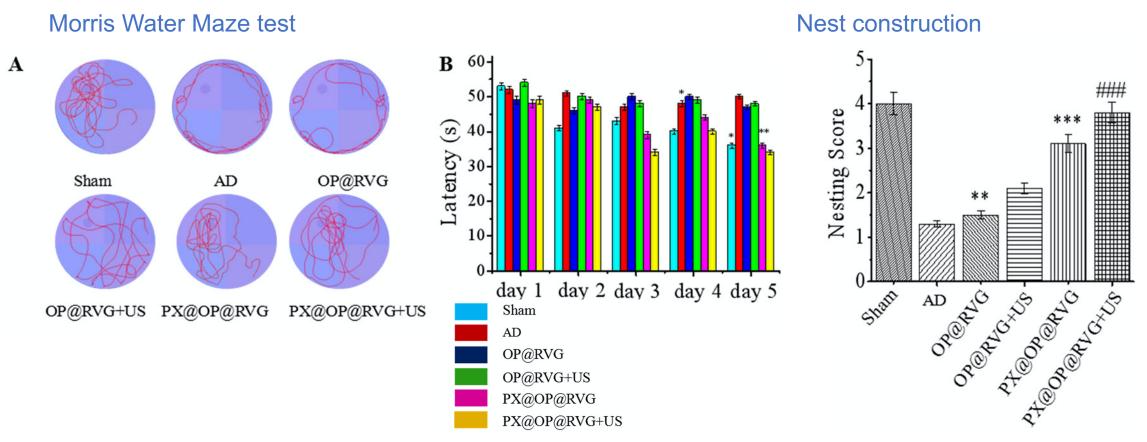


NPs effect in AD mice model



Treatment with NPs downregulated tau hyperphosphorylation.

Rescue of memory deficits



PX@OP@RVG group showed improved learning ability.

Nest construction test showed similar results.

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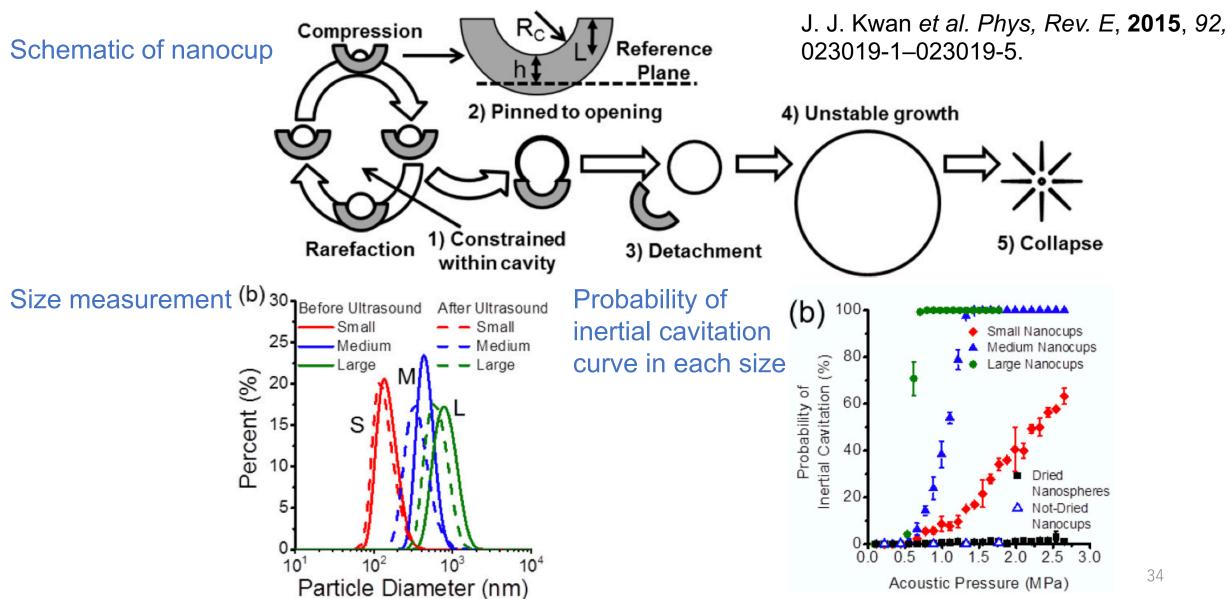
Summary

Summary

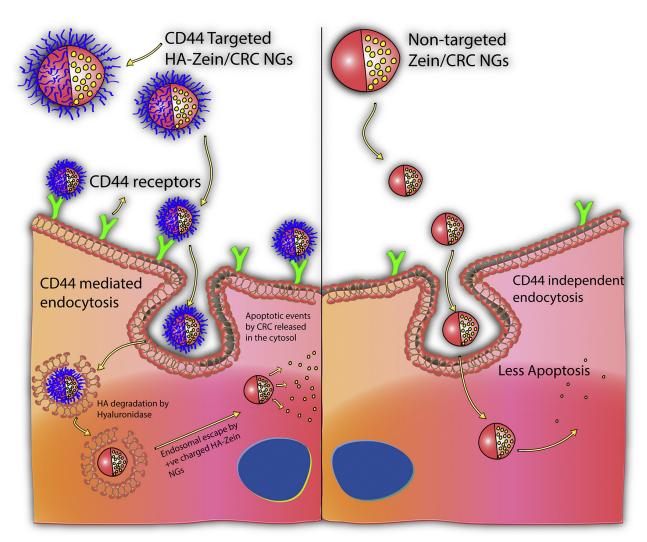
- SDT is a novel non-invasive therapeutic modality.
- NPs enhances therapeutic effect of SDT.
- BBB opening by UTMD can solve the main problem of drug delivery system.
- NP-augmented SDT can be applied to not only cancer but also Alzheimer disease.

Appendix

Nanocup decreases cavitation threshold (P12)



CD-44 targeting by hyaluronic acid (HA)

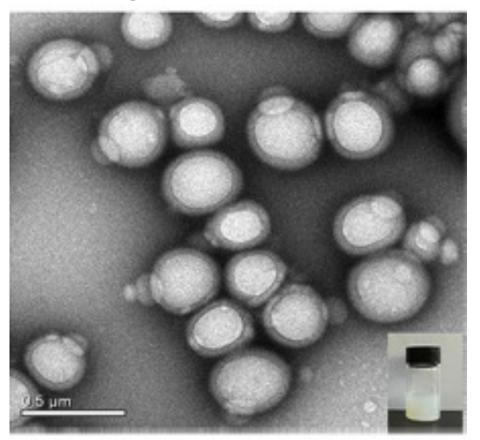


 HA recognize CD-44 receptors, which are overexpressed in tumor cells.

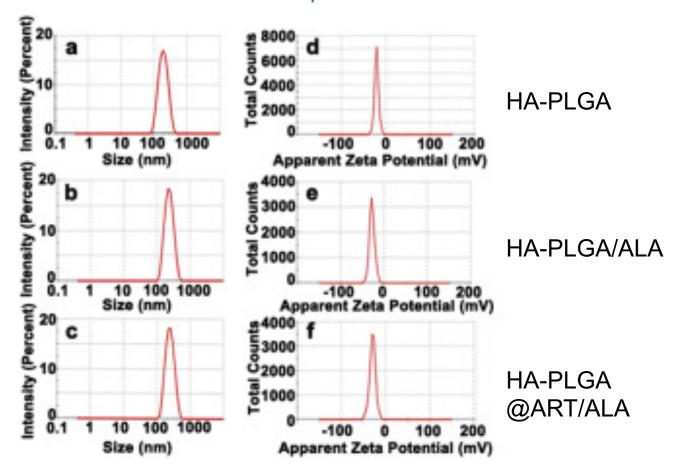
 NPs are then internalized via CD-44 mediated endocytosis.

Characterization of NPs (P14–P19)

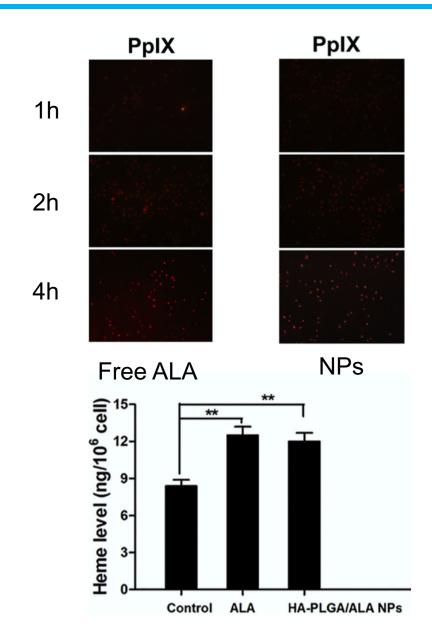
TEM image



Size distribution & Zeta potential



Cellular uptake and heme level (P14–19)



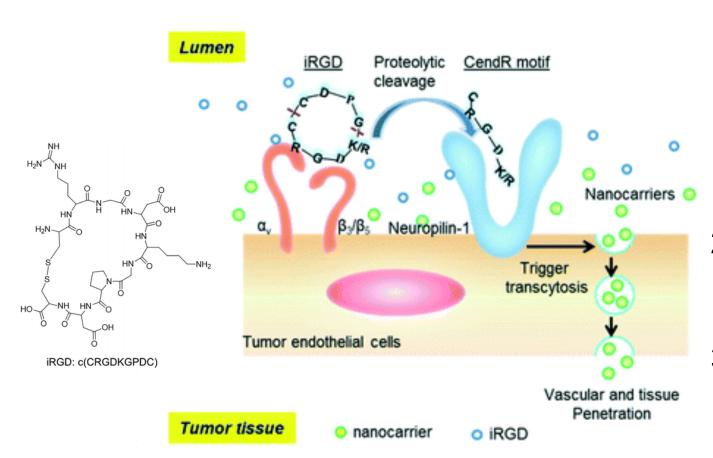
ALA is a precursor of PpIX, which shows red-fluorescence.

There was no remarkable difference between ALA and NPs.

→NPs could enter cells efficiently.

Both ALA and NPs increased heme level.

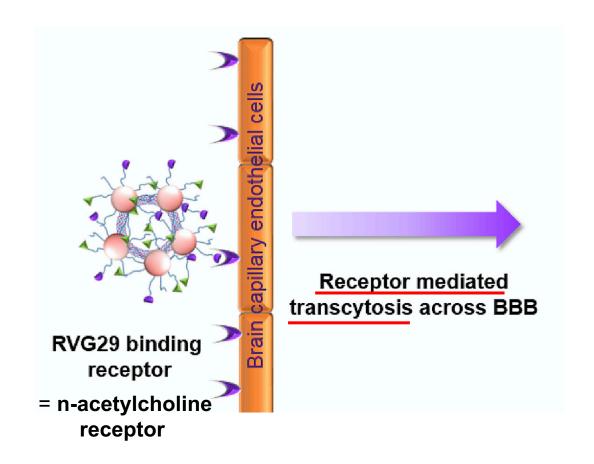
Tumor targeting by iRGD (P22)



- 1. iRGD sequence binds to $\alpha v \beta_{3/5}$ integrin, which are specifically expressed in tumor vessels or tumor cells.
- iRGD is hydrolyzed by host protease to expose CendR motif.
- 3. CendR interacts with neuropilin to initiate internalization.

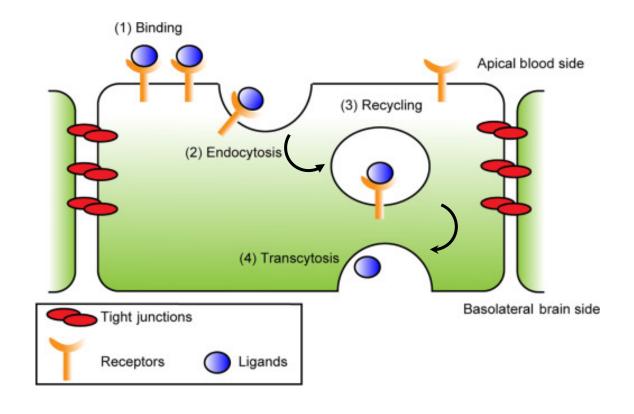
Rabies Virus Glycoprotein (RVG) drug delivery (P27)

The scheme of drug delivery by RVG peptide



Yang Liu et al. Biomaterials, 2016, 80, 33-45.

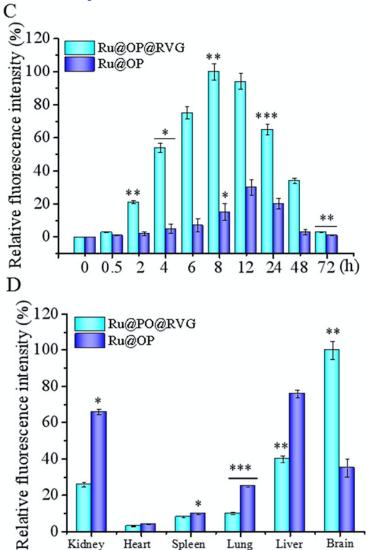
Receptor mediated transcytosis



Zhui Zhang, Changyou Zhan, Brain Targeted Drug Delivery system, 2019, 105–128.

NP biodistribution (P26–30)

Quantitative analysis for the fluorescence in vivo



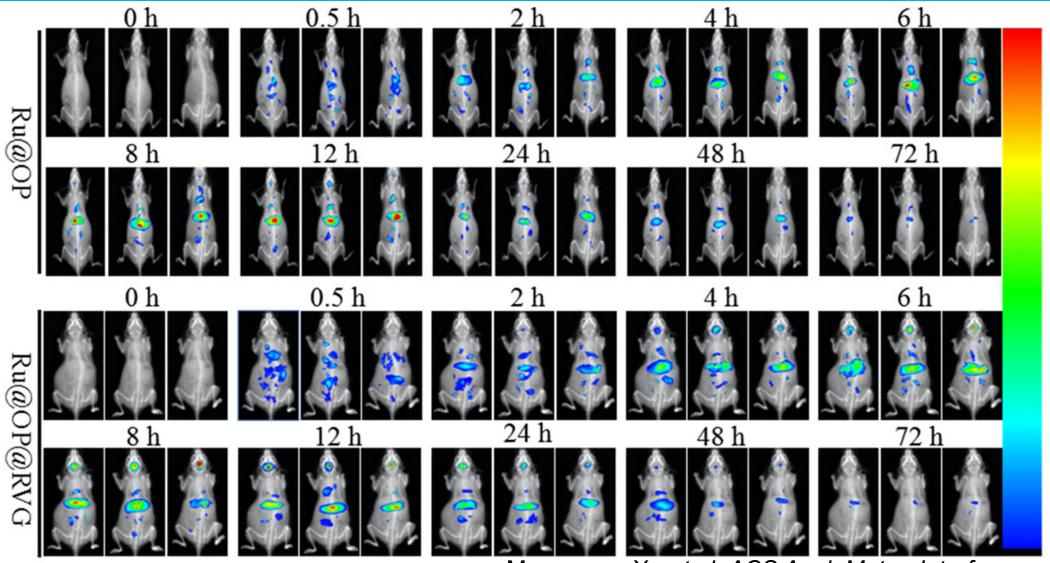
RVG-modified NPs had better circulation and retention efficiency.

NPs remarkably accumulated in the brain.

→RVG active targeting and improved penetration of BBB

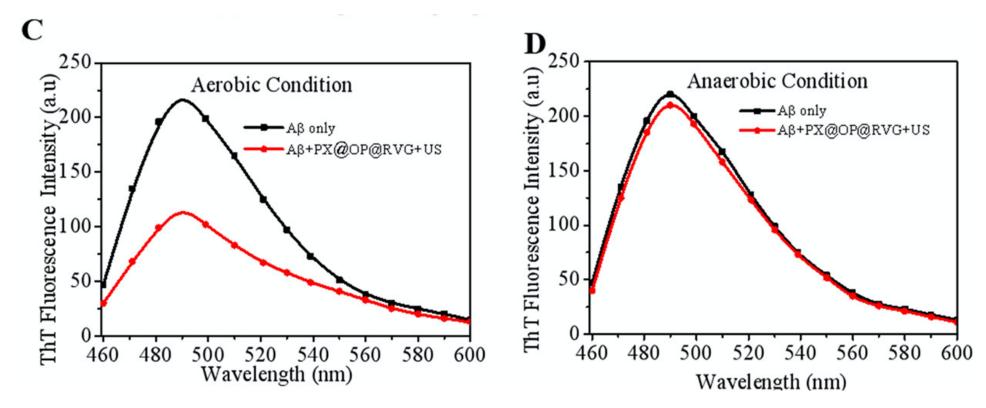
Mengmeng Xu *et al. ACS Appl. Mater. Interfaces*, **2018**, *10*, 32965–32980.

NP biodistribution (P26–30)



Mengmeng Xu *et al. ACS Appl. Mater. Interfaces*, **2018**, *10*, 32965–32980.

Inhibition of $A\beta$ aggregation (P28)

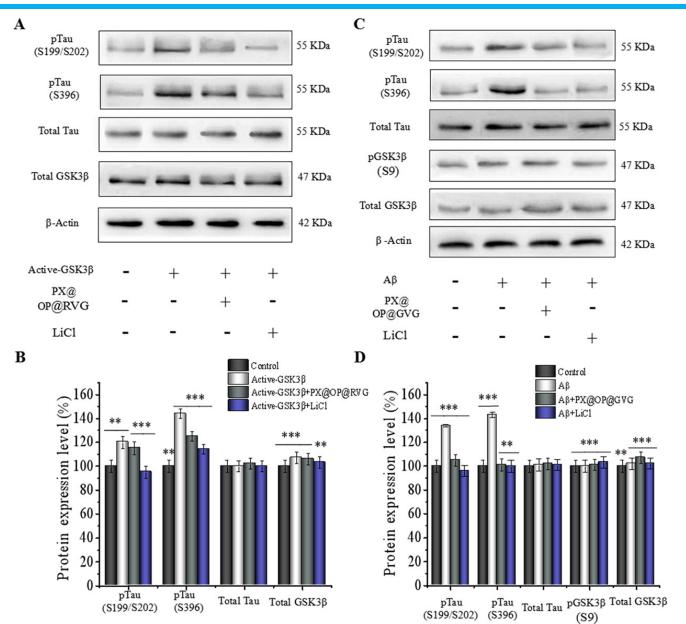


Anaerobic condition → None ROS production

ROS generation contributes to the inhibitory effect of US excited PX@OP@RVGs on A β aggregation.

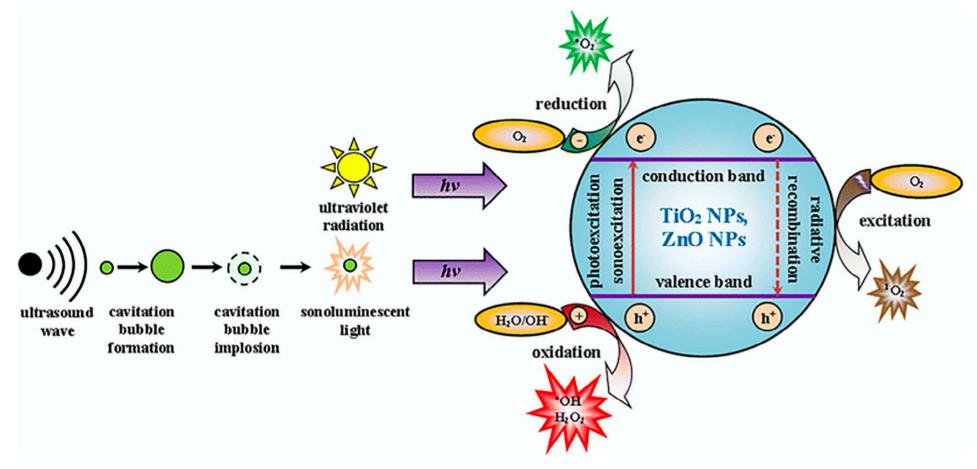
Mengmeng Xu *et al. ACS Appl. Mater. Interfaces*, **2018**, *10*, 32965–32980.

Inhibition of tau hyperphosphorylation (P29)



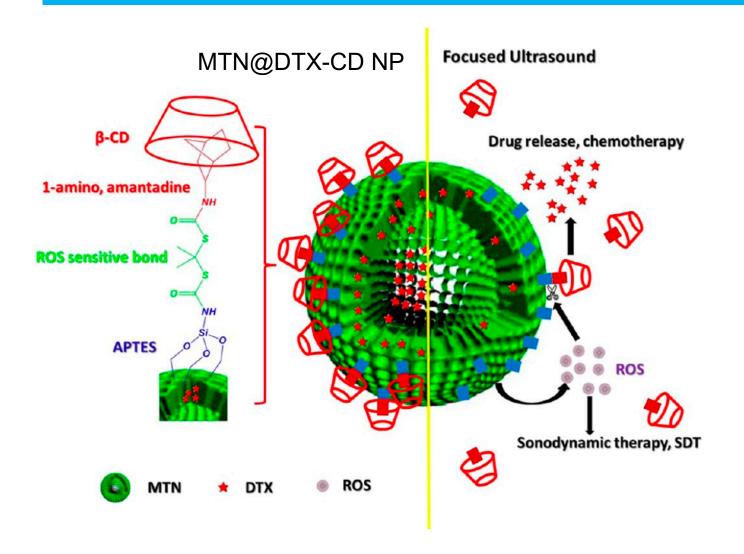
Mengmeng Xu et al. ACS Appl. Mater. Interfaces, 2018, 10, 32965–32980.

Inorganic sonosensitizer



Not only organic molecules but also inorganic NPs such as TiO₂, ZnO, etc. act as a sonosensitizer.

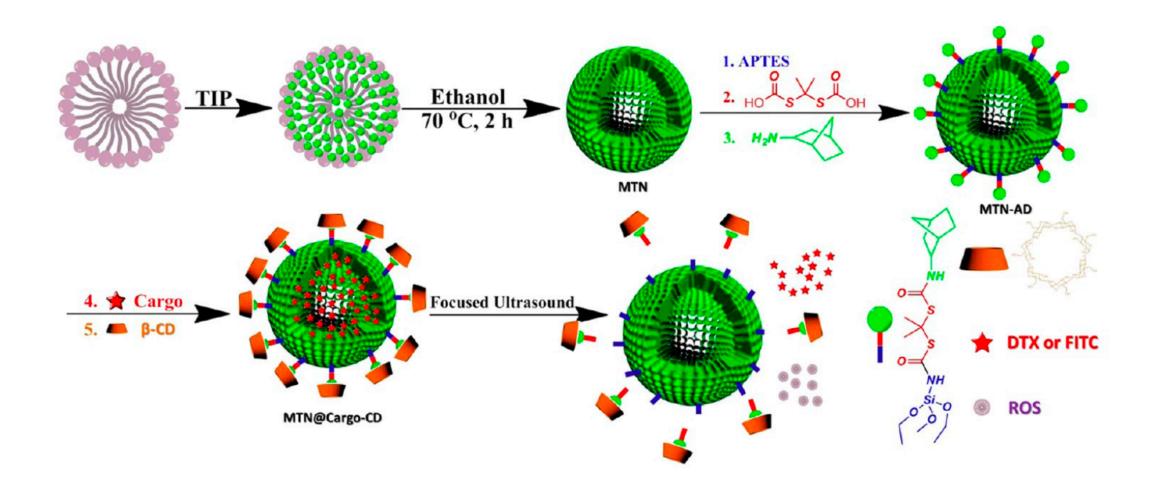
Mesoporous titanium nanoparticle loading DTX



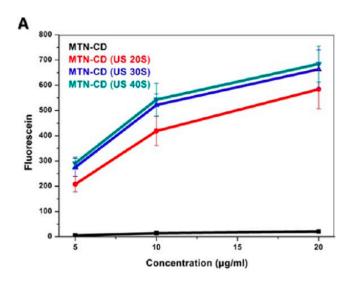
- Mesoporous TiO2 NPs (MTN):
 Carrier and sonosensitizer
- Docetaxel (DTX):
 Anti-cancer drug, loaded in pores
- β-cyclodextrin (β-CD):
 A bulky gatekeeper to block mesopores

<u>US-triggered drug release</u> by ROS sensitive linker

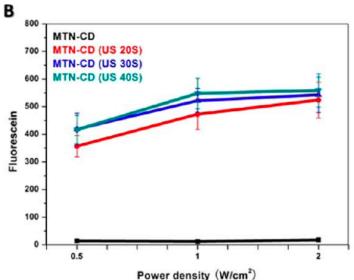
Synthesis of MTN@DTX-CD NPs



¹O₂ generation ability

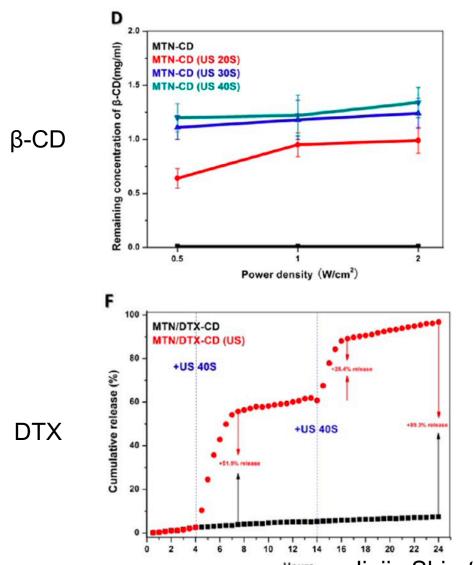


¹O₂ production was more efficient with increased concentration of MTN-CD.



US power density and irradiation time were also important.

US-triggered drug release



β-CD disperse showed the cleavage of ROS-sensitive linker was occurred.

Rapid increase of DTX after US irradiation.

- 51.9% increase (4~7.5 h)
- 28.4% increase (14~17 h)

Cell apoptosis assay

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Average	percentages

Cusums	Quadrant statistics (MCF-7 cells)			
Groups	health	necrotic	apoptosis	
Control	96.8±0.3	0.3±0.02	2.9±0.1	
Control+US	92.2±2.1	4.5±1.1	3.3±0.3	
MTN-CD	95.8±1.1	1.1±1.7	3.1±1.5	
MTN-CD+US	47.3±3.9	8.1±1.4	44.6±4.1	\leftarrow SDT only
DTX	68.9±2.1	1.8±0.3	29.3±0.9	← chemotherap
MTN@DTX-CD	82.2±4.4	1.9±1.1	15.9±4.4	
MTN@DTX-CD+US	29.7±4.9	6.8±3.2	53.5±4.4	\leftarrow SDT + chem

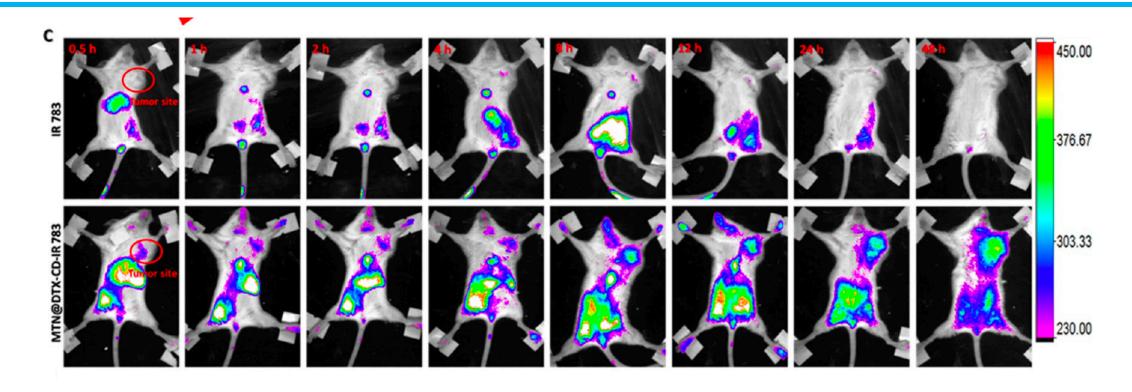
apy only

notherapy

MTN@DTX-CD with US showed higher effect than the others.

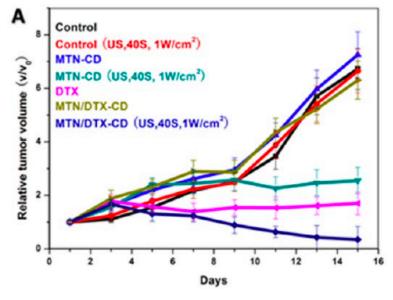
→The combination of SDT & chemotherapy led to more apoptosis.

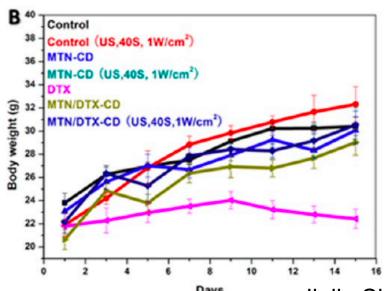
In vivo studies



- Tumor targeting and accumulation
- Long circulation ability

In vivo studies





MTN-CD+US: SDT

DTX: chemotherapy

MTN/DTX-CD+US: the combination of SDT & chemotherapy

→More effective and less toxic side effect